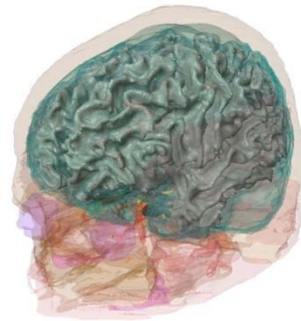


Models for tDCS



Marom Bikson

Lucas Parra, Abhishek Datta, Mathias Hueber

Neural Engineering Laboratory - Department of Biomedical Engineering

The City College of New York of CUNY, New York, NY

\$ NIH, Wallace Coulter Foundation, DoD

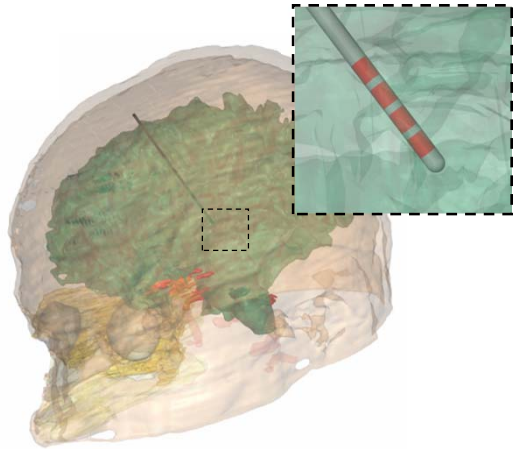
Neuralengr.com

Why Neuromodulation?

(applying electricity to CNS to treat neuropsychiatric disorders and enhance recovery)

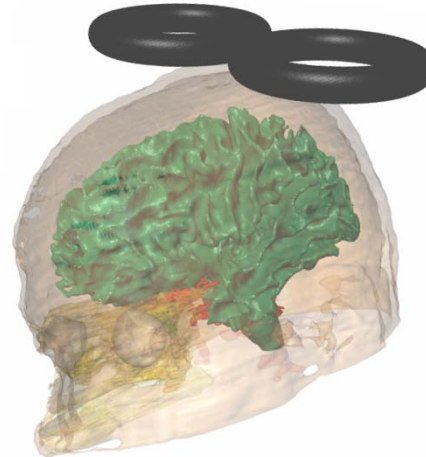
- **Application/outcome specific** (neuropsychiatric, rehabilitation, cognitive performance...)
- **Individualized therapy** (customize, tune-able)
- **Targeted brain modulation** (space + time)
- **Safe** (reversible, no residue, minimal complications + counter-indications)
- **Cost / Access** (multi-use, production, treatment-infrastructure)

Types of Brain Neuromodulation (efficacy and safety)



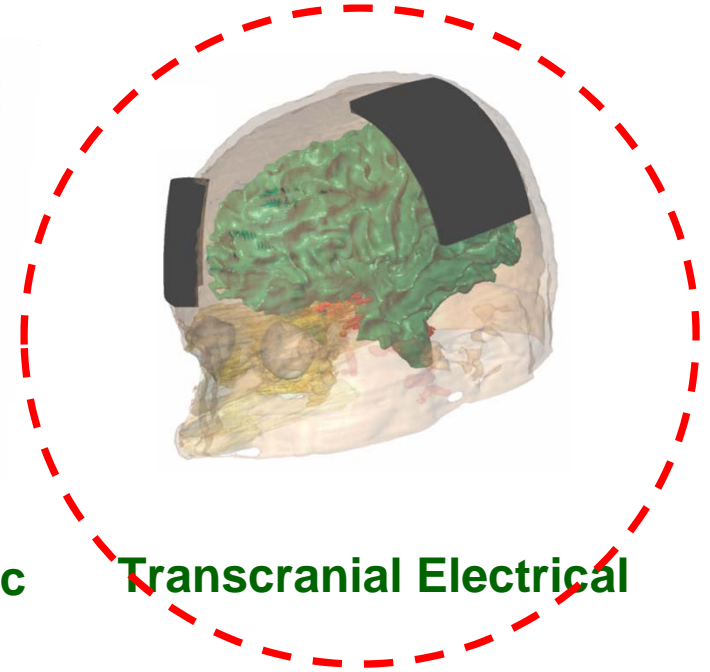
Invasive Leads
(also Vagus, Spinal..)

- Very Targeted
- Safety + Reversibility Concerns
- Supra-threshold dose only
- Costly (resources)



Transcranial Magnetic

- Somewhat Targeted
- Mostly Safe (clinic)
- Supra-threshold dose only
- Not cheap (resource)



Transcranial Electrical

- ~~Not Targeted~~
- Safe
- Any dose, Supra- or Sub-threshold
- Cheap (home)

Computational models are critical tools for clinicians to understand and improve the outcomes of Neuromodulation

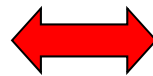


Models are ONLY useful to make predictions

Critical issue of “dose”

Computational models predict the electric field generated in the brain for a *specific* stimulation configuration/settings

**Electrical activity
(efficacy and safety) is
determined by electric
fields at tissue**

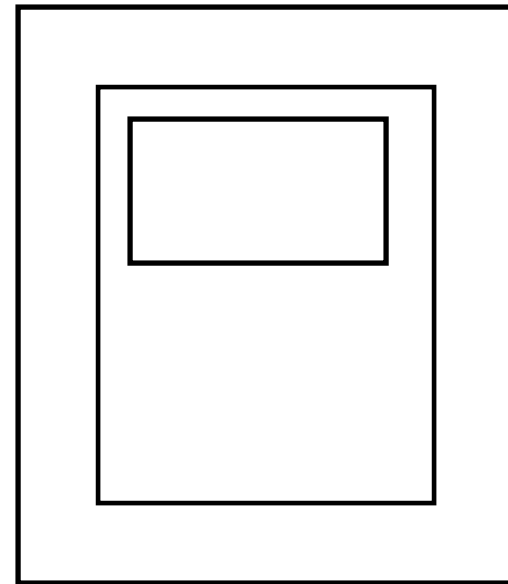


**Clinical dose is set by
systemic application
(stimulators and
pads/coils)**

2 steps of “Forward” models

1) Divide the head into compartments
(skin, skull, CSF, brain....)

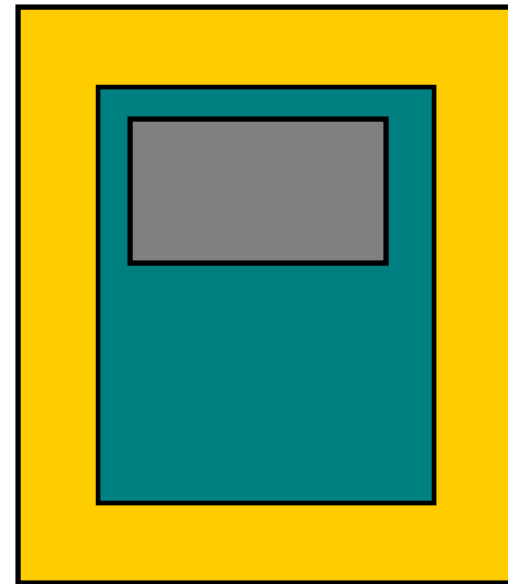
2) Apply electricity
(the way is it applied clinically)



2 steps of “Forward” models

1) Divide the head into compartments
(skin, skull, CSF, brain....)

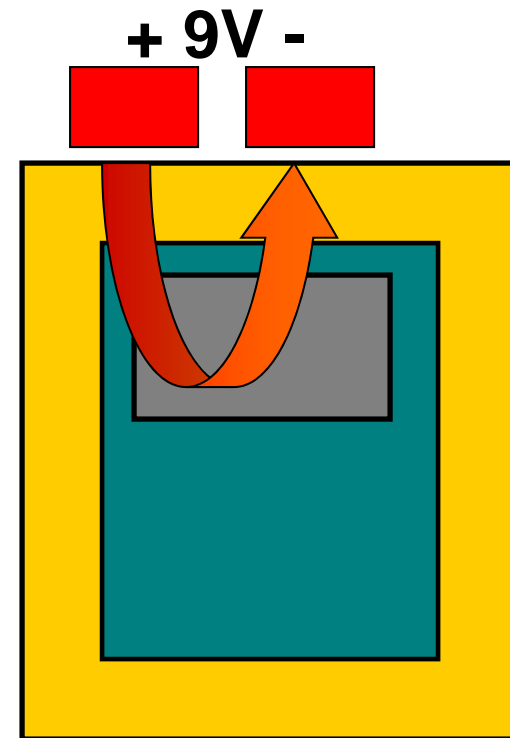
2) Apply electricity
(the way is it applied clinically)



2 steps of “Forward” models

1) Divide the head into compartments
(*skin, skull, CSF, brain....*)

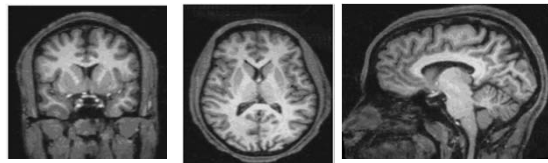
2) Apply electricity
(*the way is it applied clinically*)



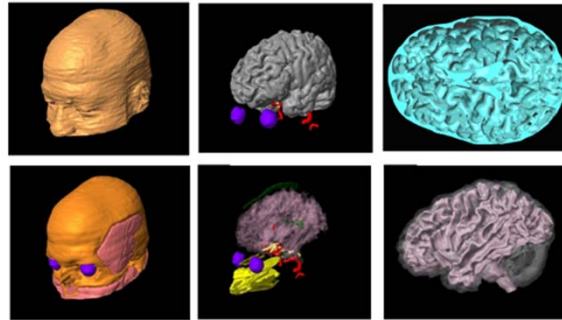
= See where the current goes in the brain !

Workflow (engineering center)

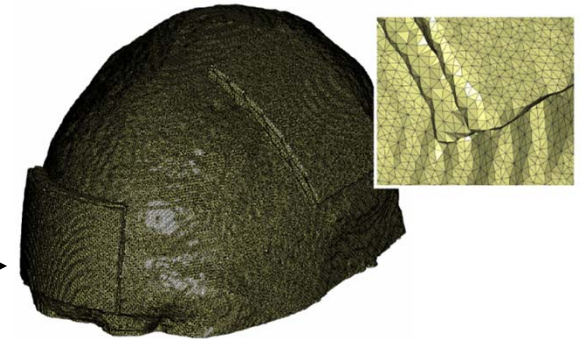
Full work-flow developed to preserve accuracy and resolution



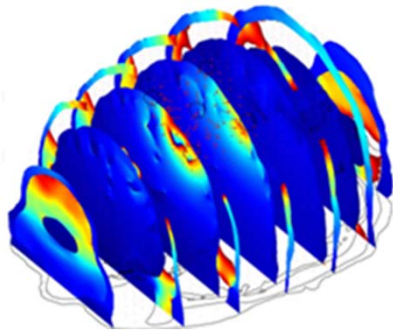
MRI sequences optimized for tDCS modeling (3T at 1x1x1 mm)



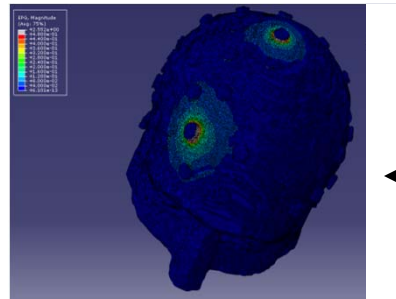
Special segmentation tools preserve resolution in generation of tissue masks



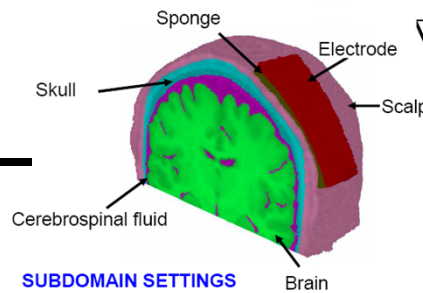
Mesh includes >10 million elements



Solution provides detail insight into brain modulation

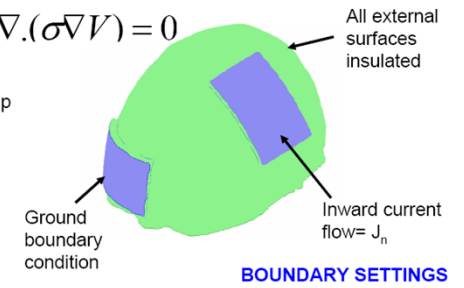


Conjugate gradient solver with <math><1E-8</math> tolerance



SUBDOMAIN SETTINGS

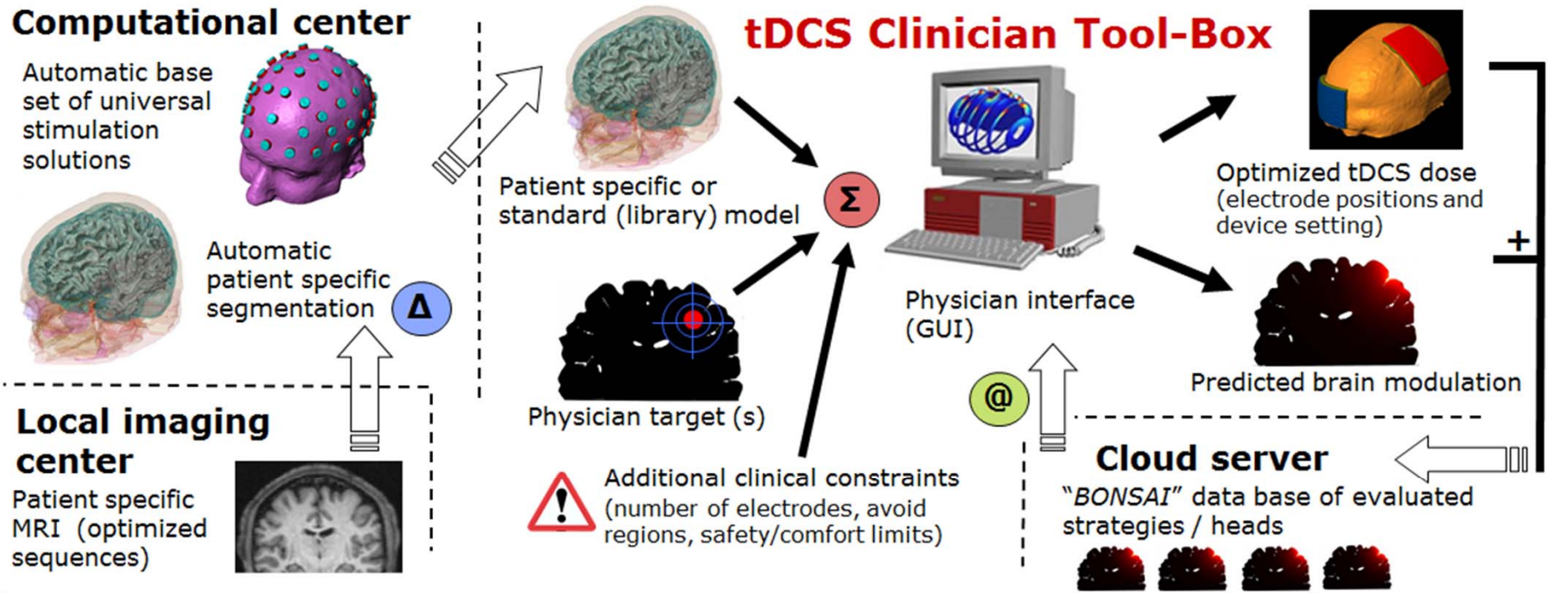
$$\nabla \cdot (\sigma \nabla V) = 0$$



BOUNDARY SETTINGS

Model physics/domains include explicit consideration of electrode properties.

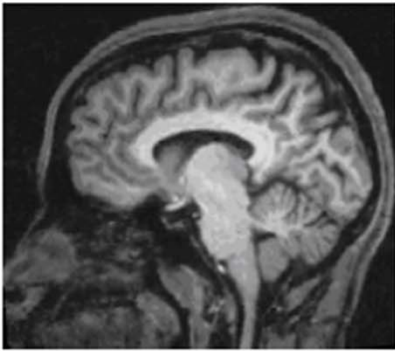
Tool-Box Workflow (clinic)



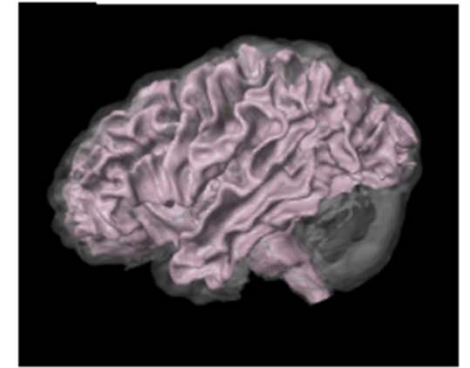
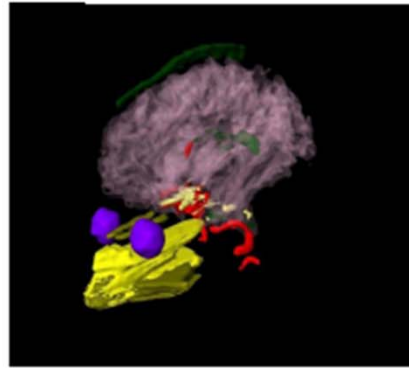
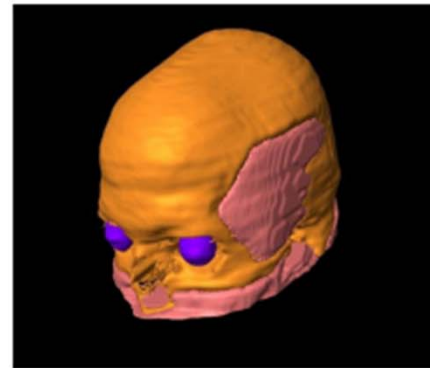
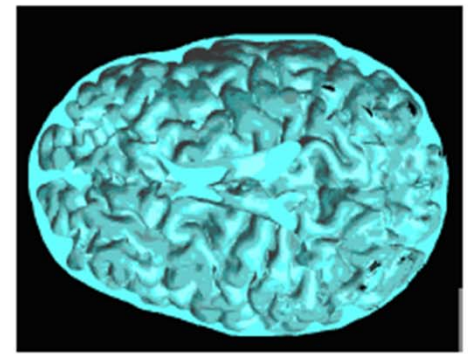
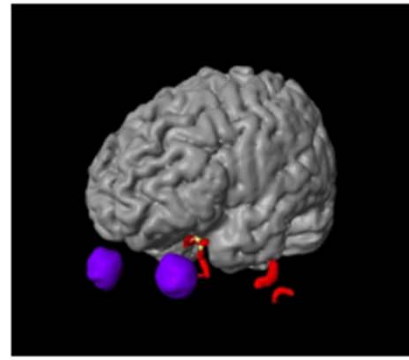
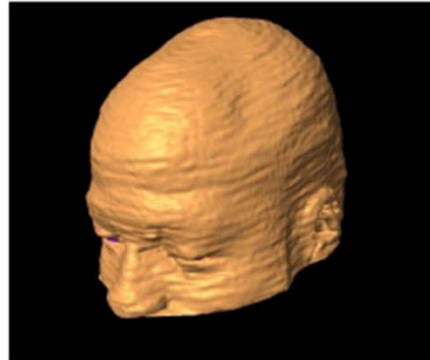
Tool-Box Engineering

- Δ Fully automatic segmentation. State-of-the-art algorithms may be regularly updated.
- Σ Optimization algorithm. Laptops exceed super-computer performance.
- @ Open-source therapy data-base and web interface.

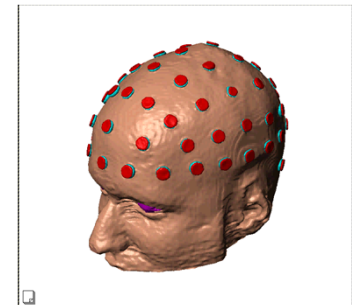
Individualized high-resolution models



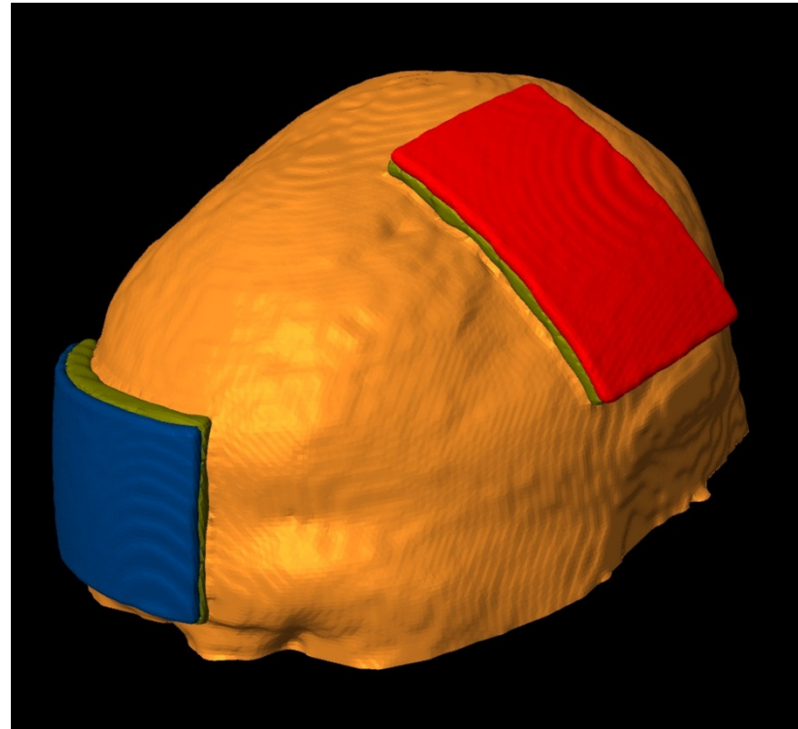
High-resolution 3T
MRI scans at 1 mm
X 1 mm X 1 mm
pixel spacing



- 1) Anatomical targeting
- 2) Customized therapy

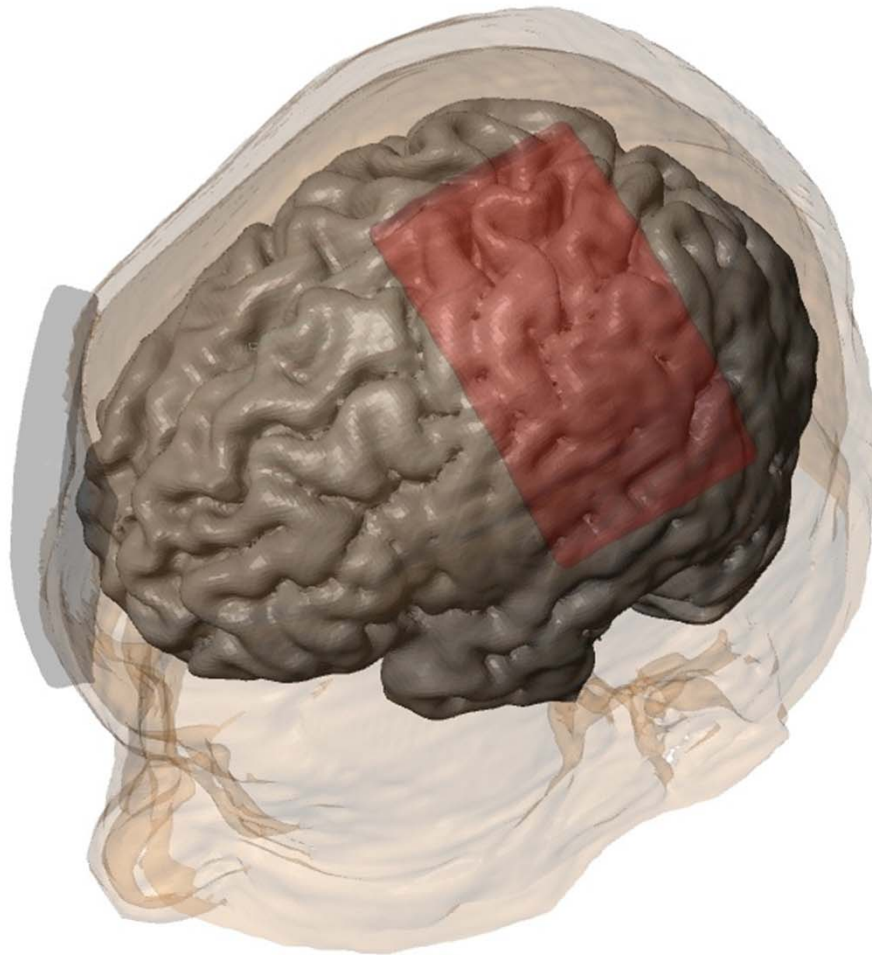


tDCS using existing and *new* electrode montages



- 1) Rapid screening and computer aided optimization
- 2) Mechanistic insight (can “look inside”)
- 3) No risk

Conventional tDCS – large pad



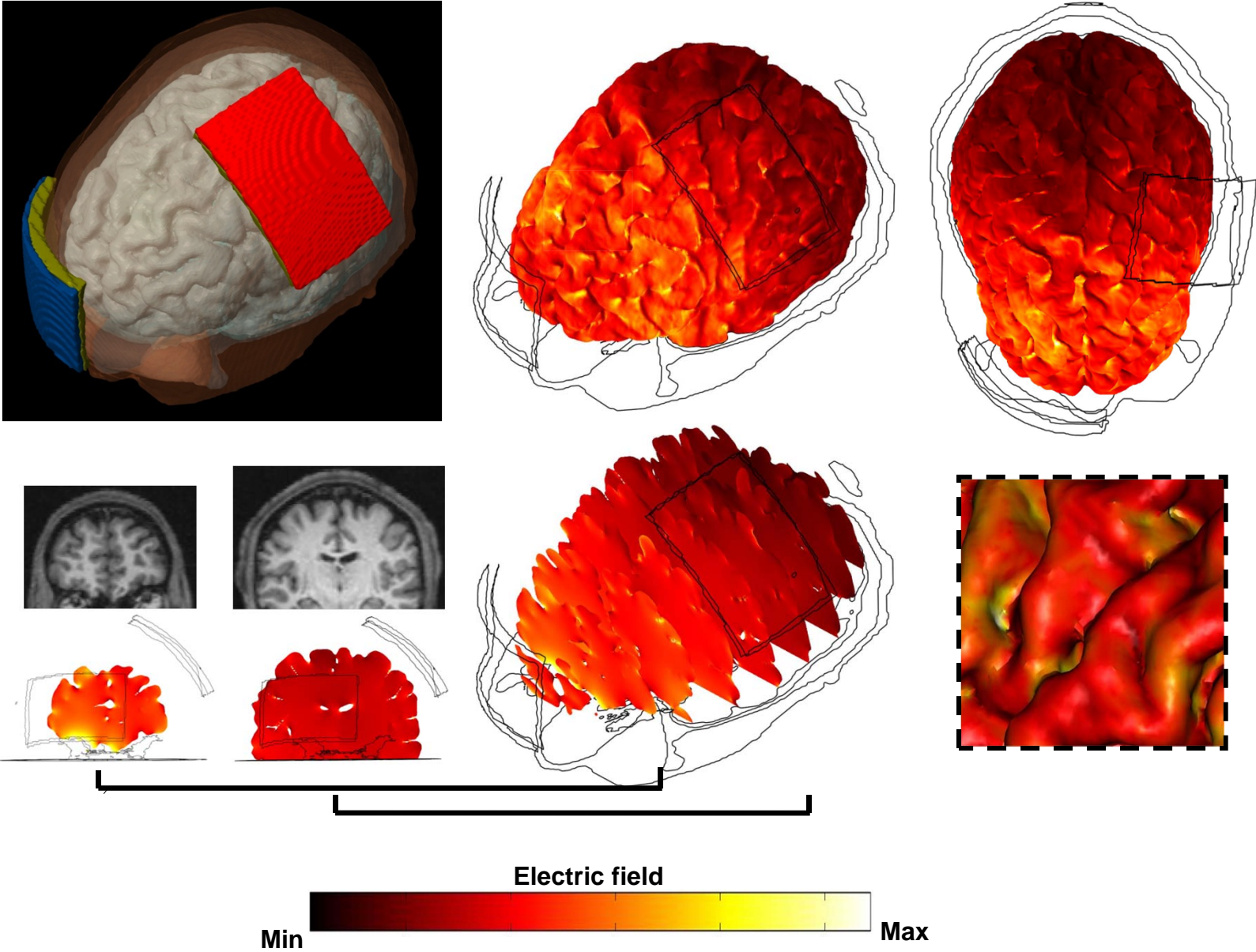
Brain Activation

Maximum

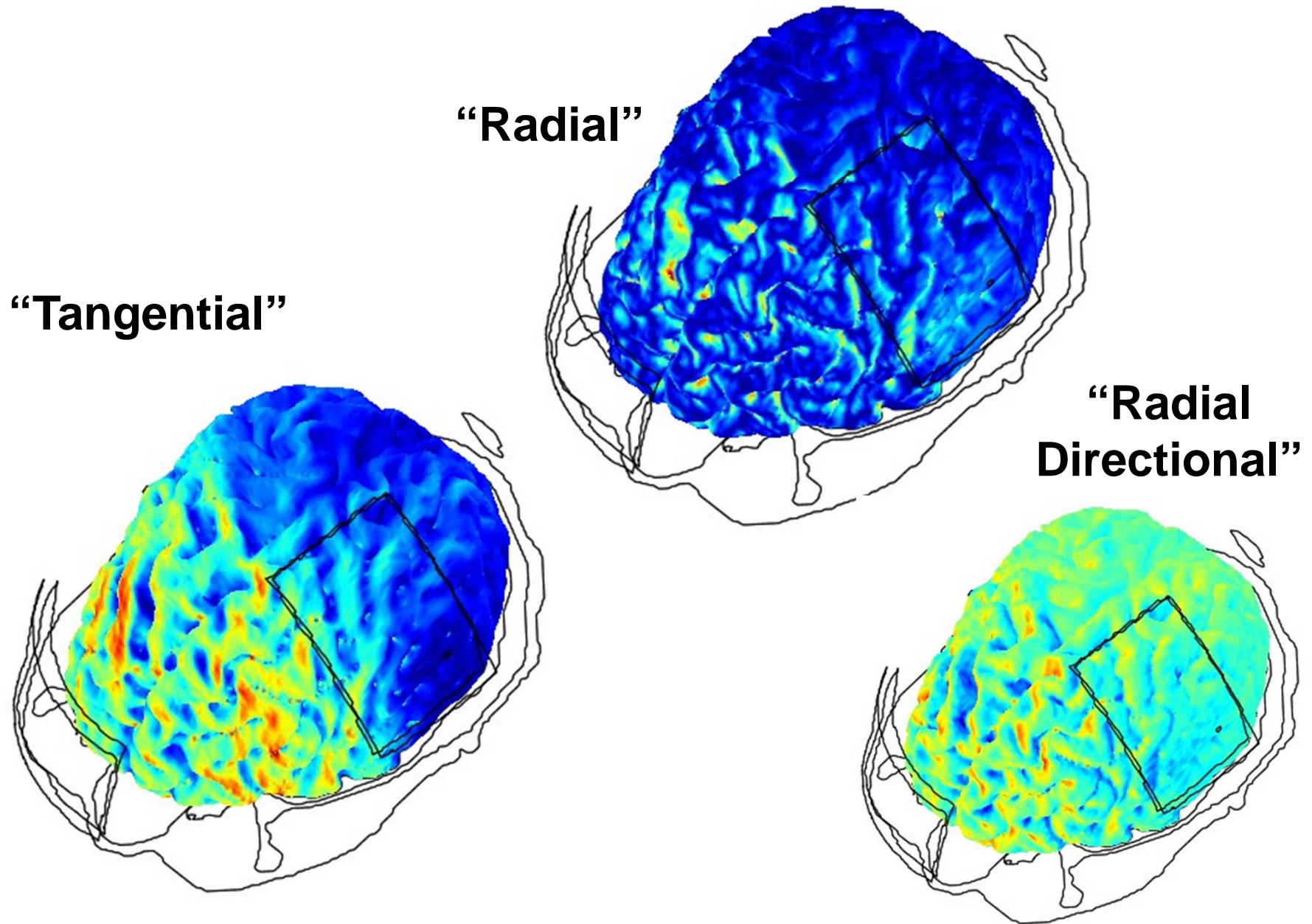
Moderate

Minimum

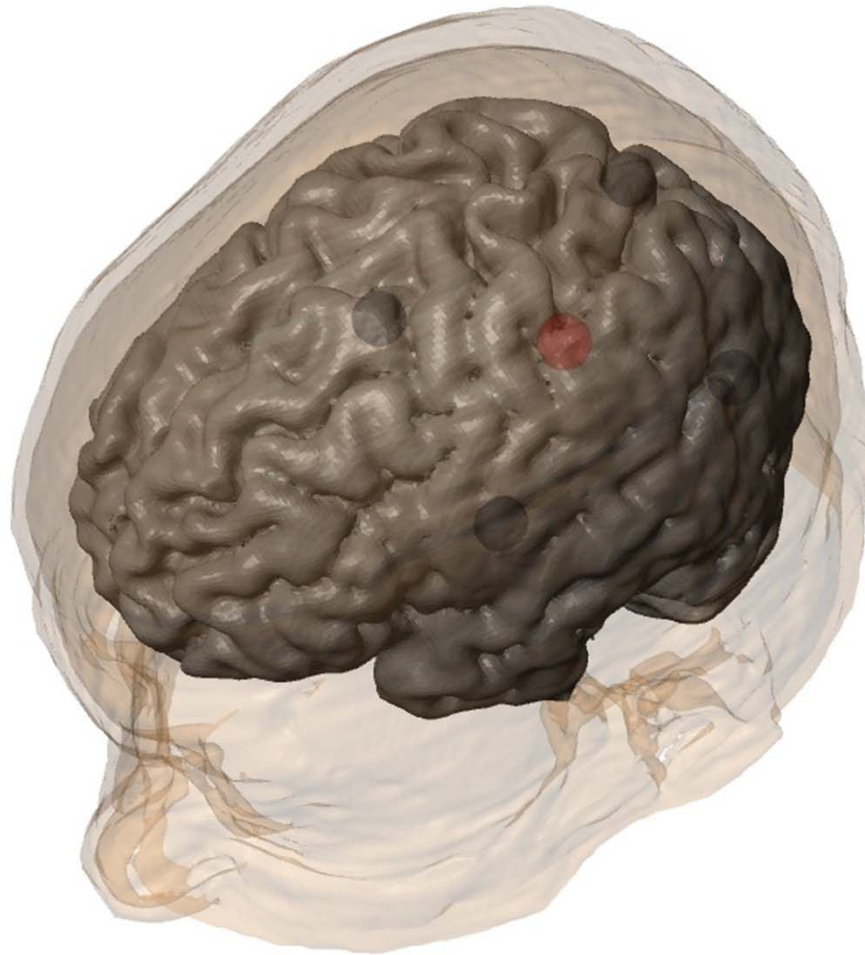
Conventional tDCS – large pad



Conventional tDCS – large pad



High-Definition tDCS – 4x1



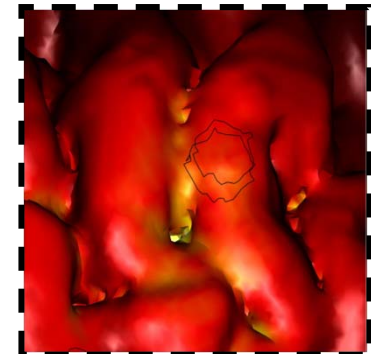
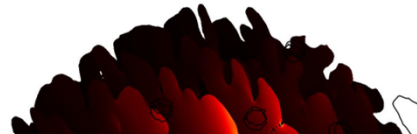
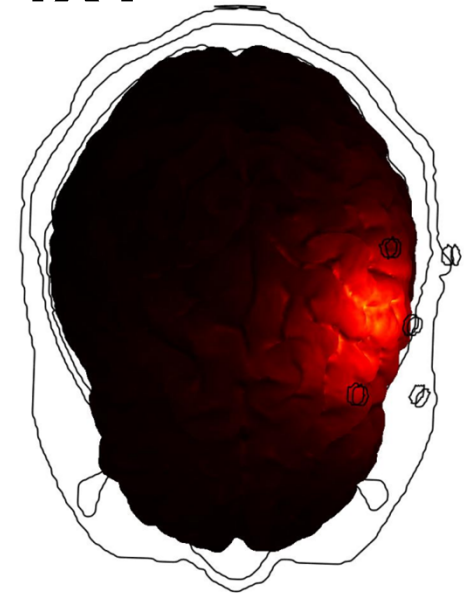
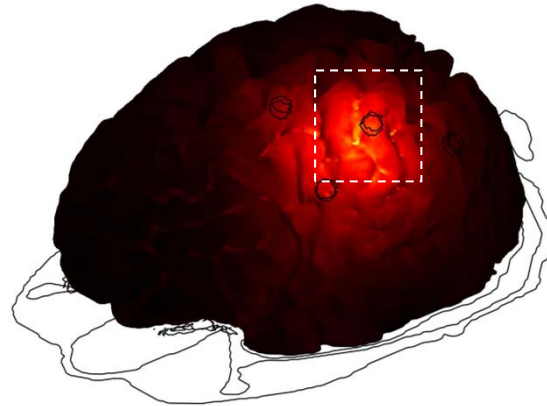
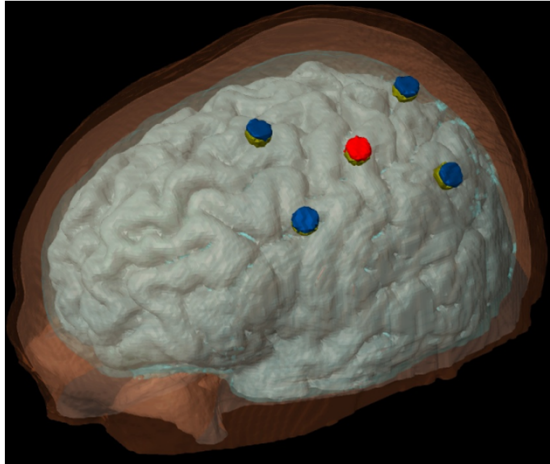
Brain Activation

Maximum

Moderate

Minimum

High-Definition tDCS – 4x1



Brain Stimulation (2009) 2, 201 7



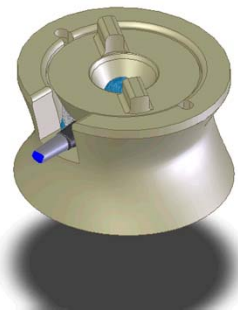
Gyri-precise head model of transcranial direct current stimulation: Improved spatial focality using a ring electrode versus conventional rectangular pad

Abhishek Datta, MS, Varun Bansal, BS, Julian Diaz, BS, Jinal Patel, MS, Davide Reato, MS, Marom Bikson, PhD

High-Definition tDCS – 4x1

Hardware Development

Soterix Medical



Clinical Trials

NIH-NINDS

*Eric Wassermann, Egas
Caparelli Dáquer*

MUSC

*Mark George
Jeff Borckardt*

Burke Rehabilitation

*Dylan Edwards
Mar Cortes*

Harvard (Spaulding)

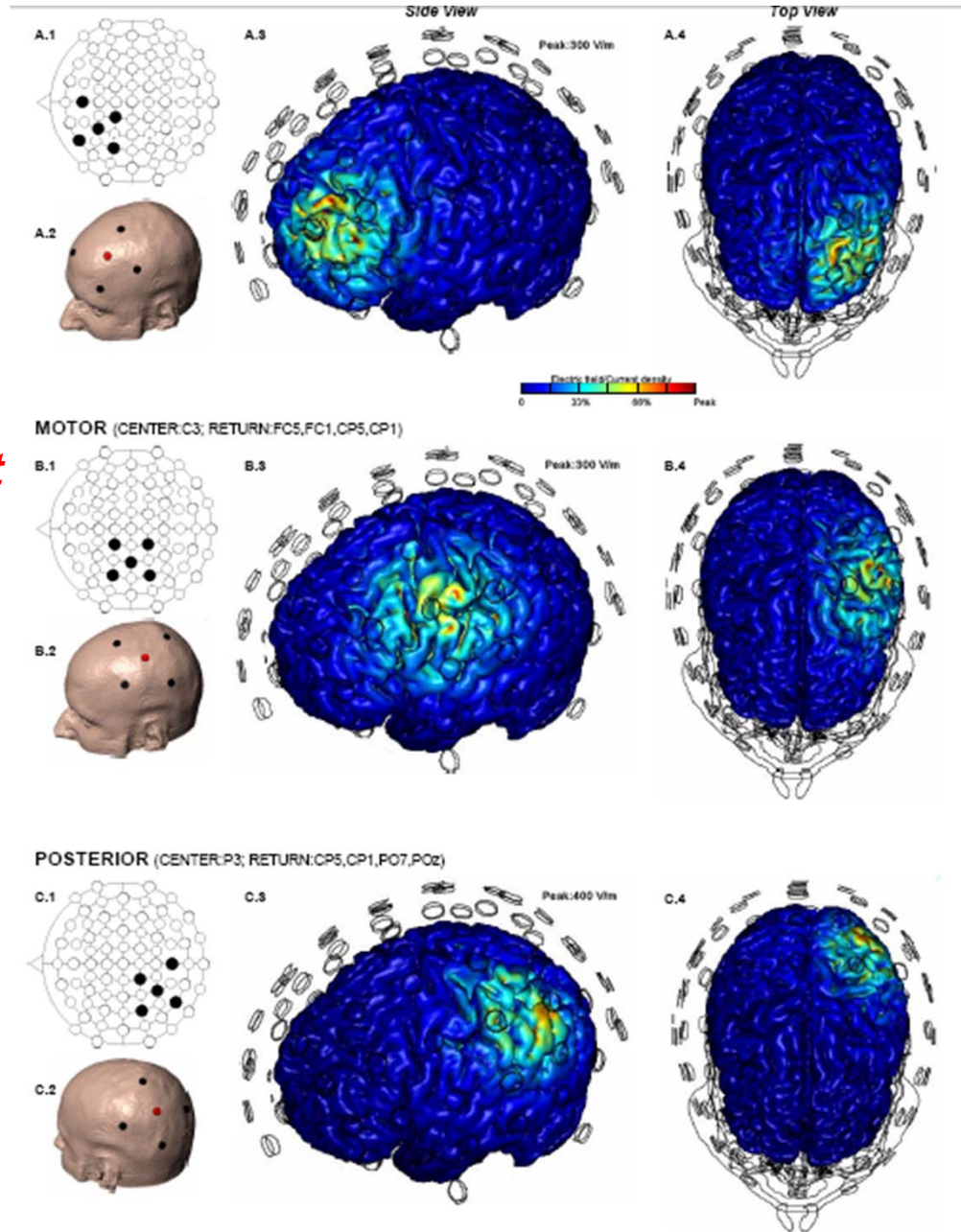
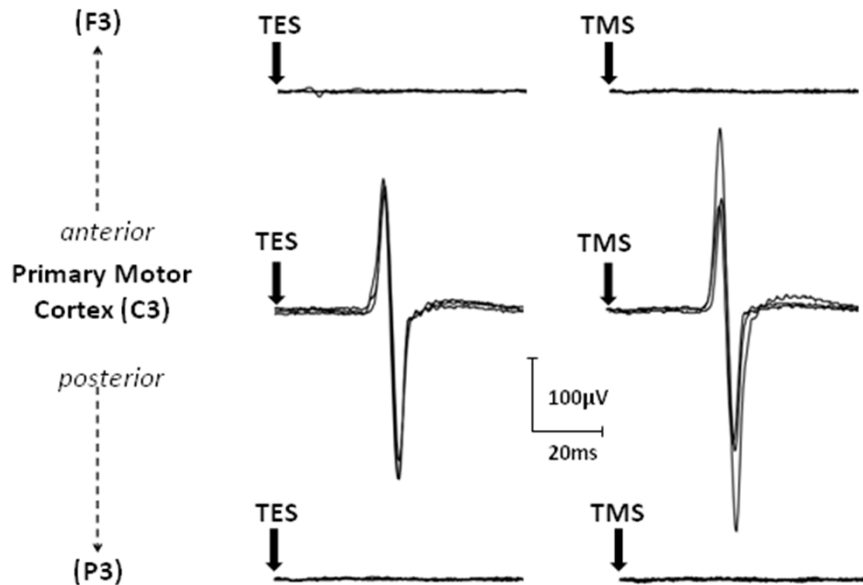
Felipe Fregni

.....

High-Definition tDCS – 4x1

Phase 1 Clinical Trials
*Burke Rehabilitation, Harvard
 Medical School*
 Dylan Edwards, Mar Cortes

**Transcranial Electrical Stimulation
 (TES) – short high-intensity pulse that
 triggers motor response (MEP)**





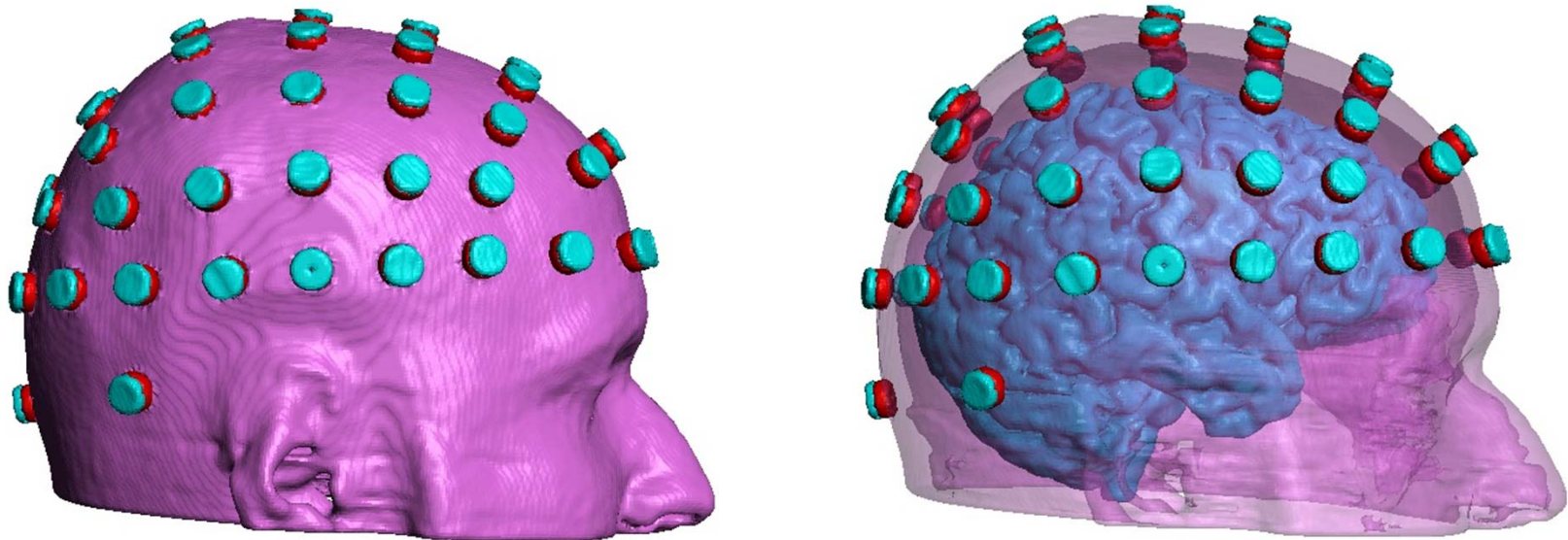
High-Definition tDCS – 4x1

**Better
Outcomes**

Design feed-back and design from clinical trials

**Models as a tool for developing
better electrotherapies**

High-Definition transcranial Electrical Stimulation (HD-tES)



4x1 HD-tDCS, 6x6 HD-tES, Deep HD-TES....

Electrode-distance dependent after-effects of transcranial direct current and random noise stimulation with extracephalic reference electrodes.

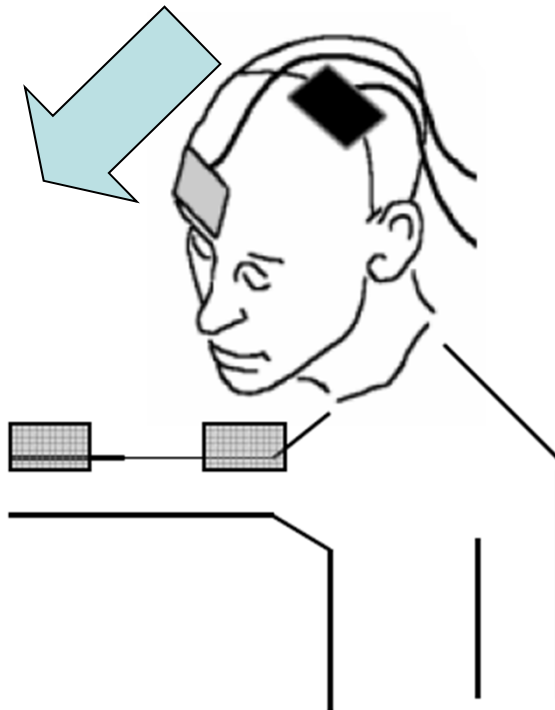
Moliadze V, Antal A, Paulus W.

Department of Clinical Neurophysiology, Georg-August University, Robert-Koch-Strasse 40, 37075 Göttingen, Germany.

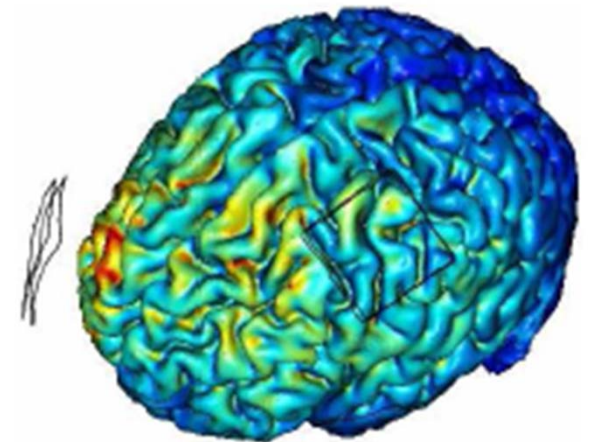
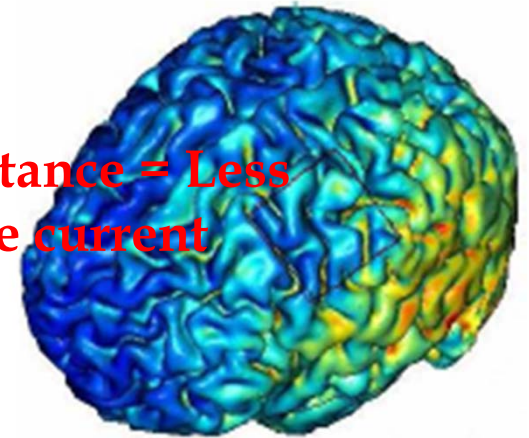
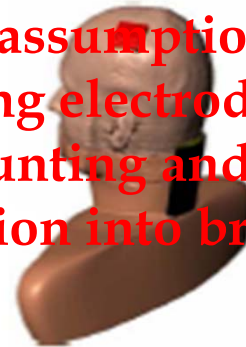


Editorial

Electrode montages for tDCS and weak transcranial electrical stimulation: Role of “return” electrode’s position and size



Clinical assumption:
Increasing electrode distance = Less scalp shunting and more current penetration into brain



?? Distance between electrode correlates *negatively* with motor cortex modulation under active electrode

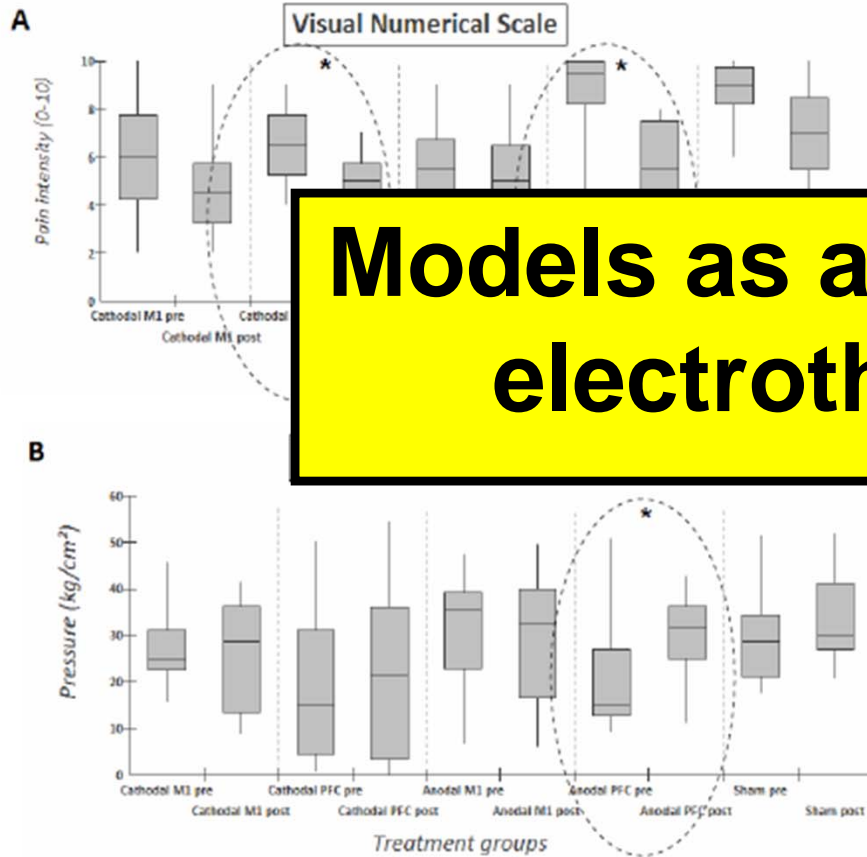


tDCS therapy design - Extracerebral electrodes in treating Fibromyalgia

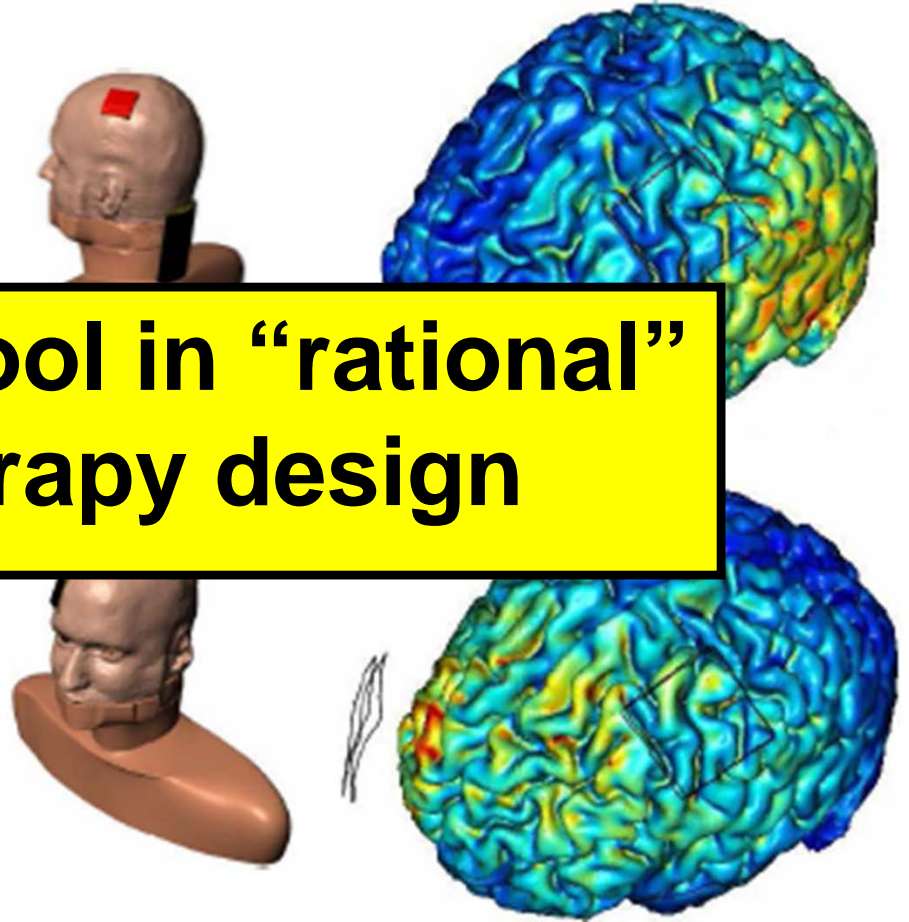
*Bahaina School of Medicine, Brazil
Spaulding Rehabilitation Hospital,
Harvard Medical School*

Editorial

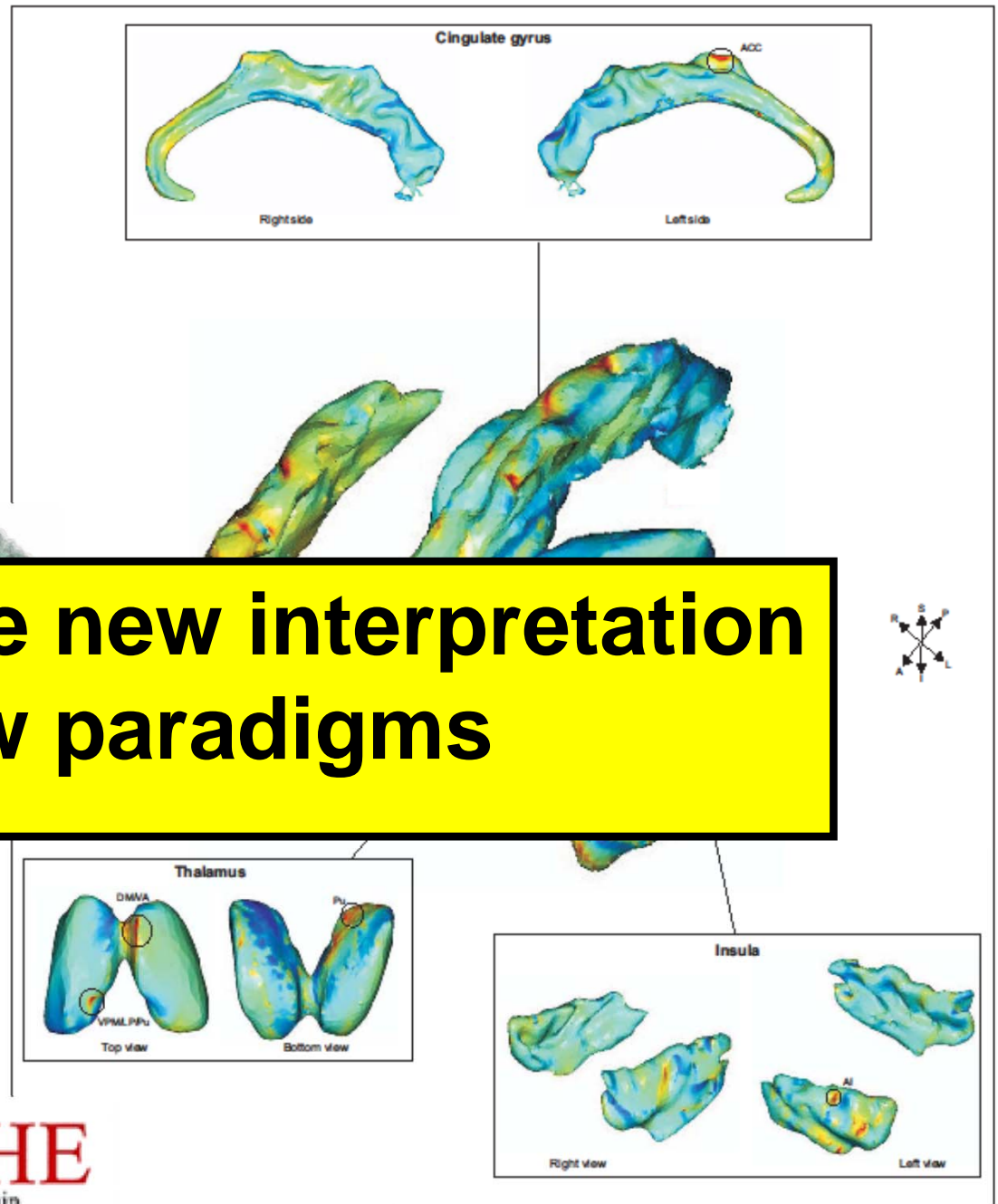
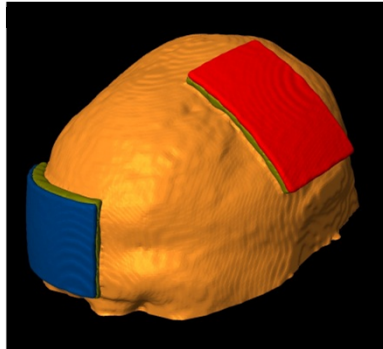
Electrode montages for tDCS and weak transcranial electrical stimulation: Role of “return” electrode’s position and size



**Models as a tool in “rational”
electrotherapy design**



Deep tDCS?



Models drive new interpretation / new paradigms

Alex DaSilva (U Michigan)
Felipe Fregni (Harvard)

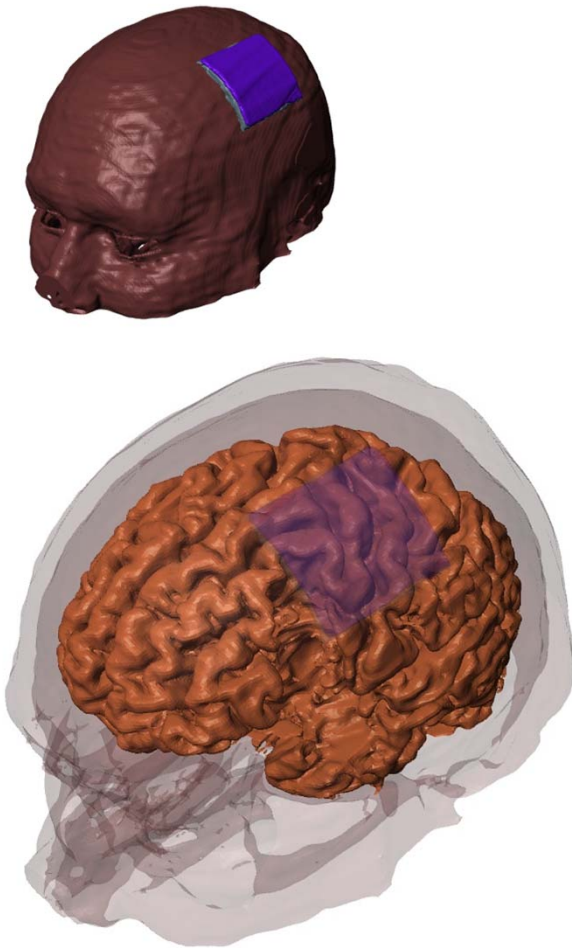
HEADACHE

The Journal of Head and Face Pain

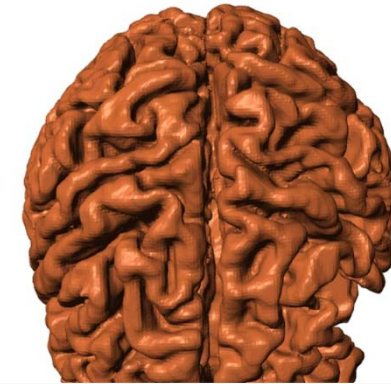
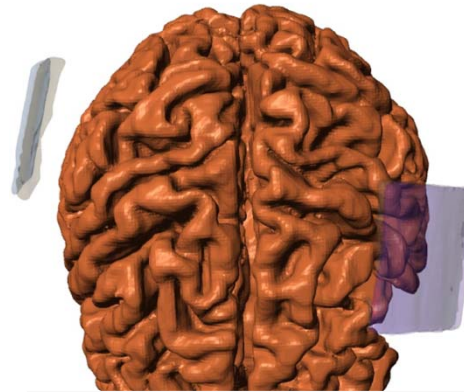
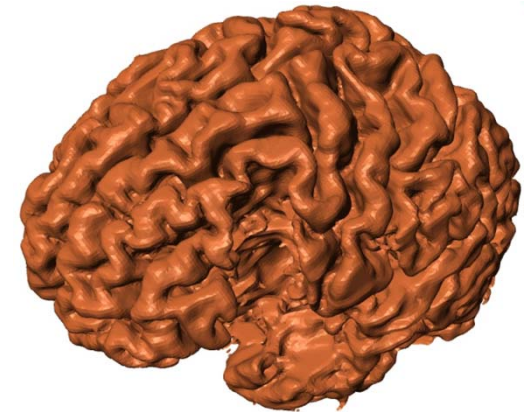
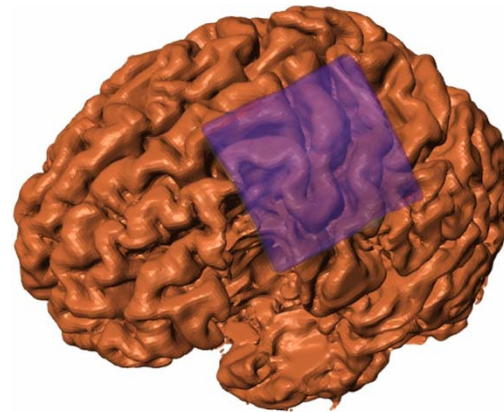
Delayed Analgesic Effects of tDCS in Chronic Migraine

tDCS for stroke rehabilitation

Julius Fridriksson
Julie Baker (USC)



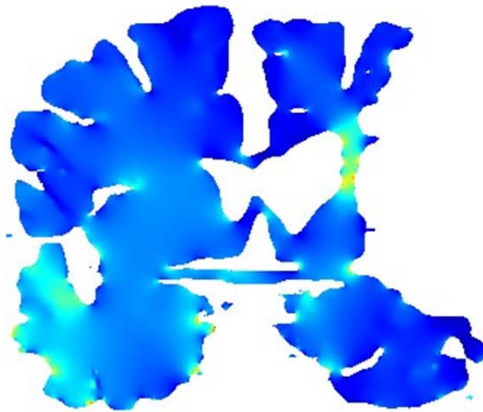
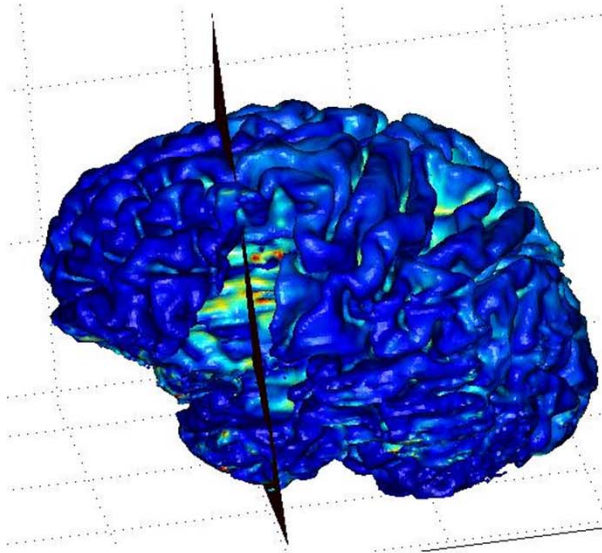
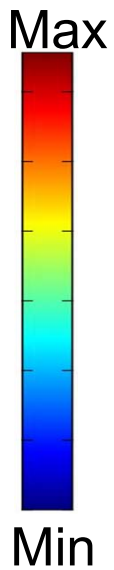
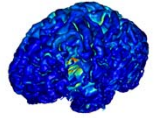
Subject X: Aphasia
Positive tDCS outcome



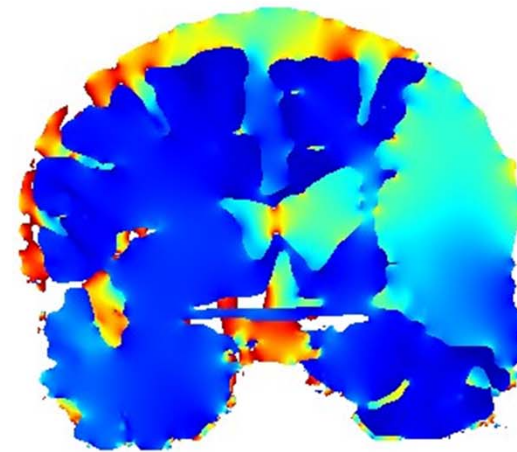
Using transcranial direct current stimulation (tDCS) to treat stroke patients with aphasia

Julie Baker, Ph.D., Chris Rorden, Ph.D., and Julius Fridriksson, Ph.D.

tDCS for stroke rehabilitation

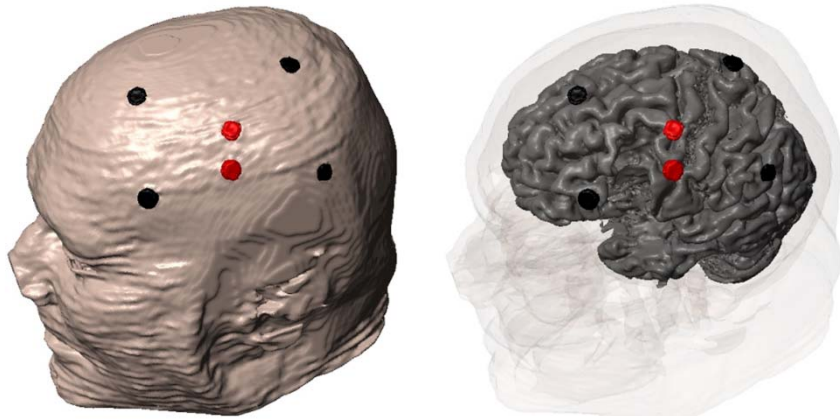


Brain Electric Field

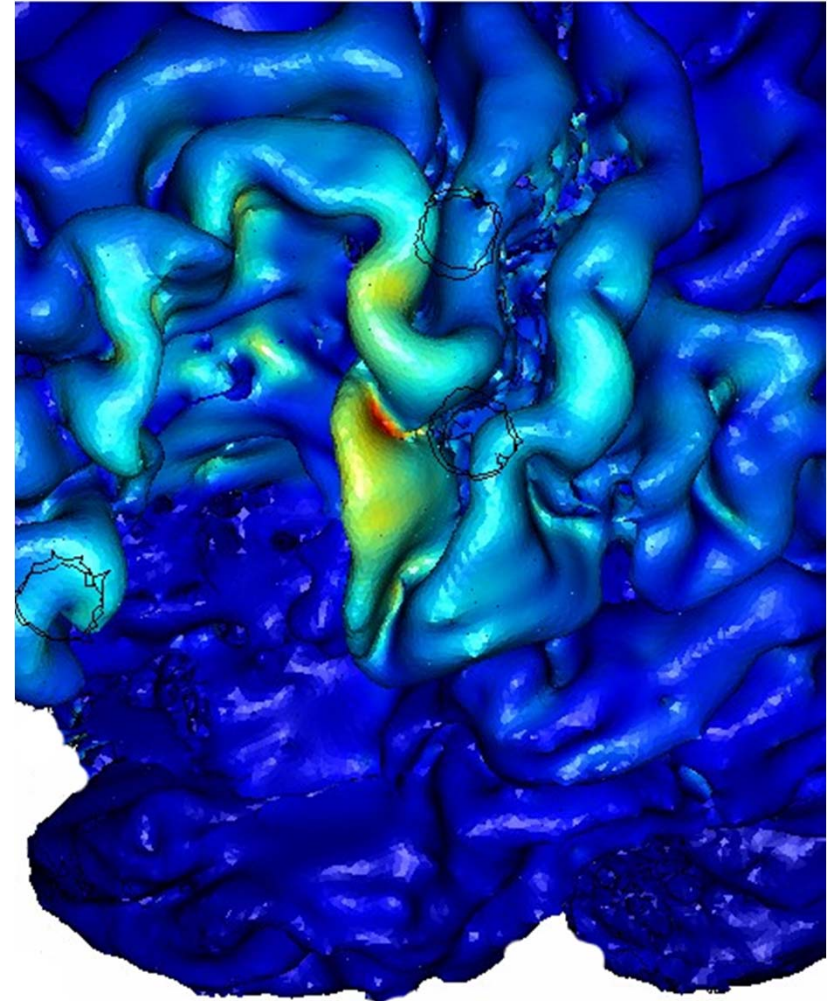
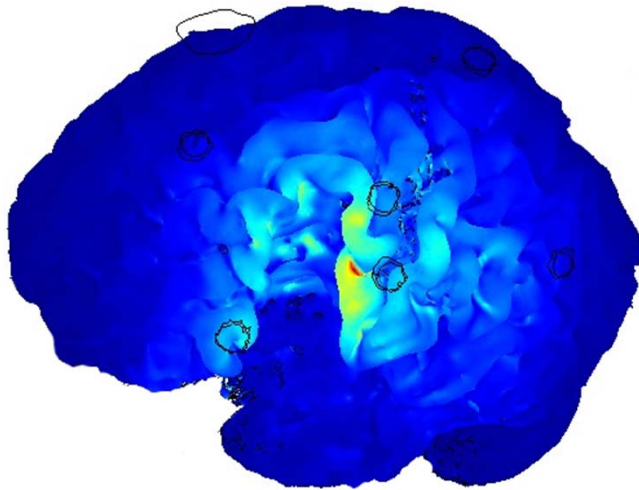


Brain and CSF Current Density

HD-tDCS for stroke rehabilitation



4x2 HD-tDCS

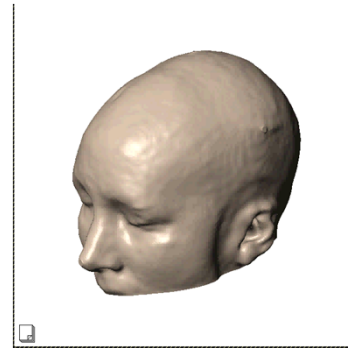


“Susceptible” Populations

**Young adults, Children...
(dose)**

Phil Defina (IBRF)

Alex Rotenberg (Boston Children’s)

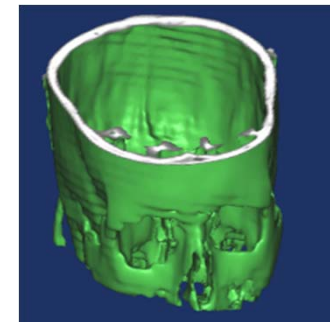


Aging....

**Procedures, implants...
(safety)**

Ziad Nahas

Mark George (MUSC)



NeuroImage 52 (2010) 1268-1278

**Skull Defects / TBI
(safety, targeting)**

Felipe Fregni (Harvard)



Contents lists available at ScienceDirect

NeuroImage

journal homepage: www.elsevier.com/locate/ynimg



Transcranial direct current stimulation in patients with skull defects and skull plates:
High-resolution computational FEM study of factors altering cortical current flow

Abhishek Datta ^{a,*}, Marom Bikson ^a, Felipe Fregni ^{b,c,*}

Engineering and modeling driving “rational” electrotherapy

Current tDCS practice

Current strategies rely on unvalidated “rules of thumb”, and incremental iterative testing

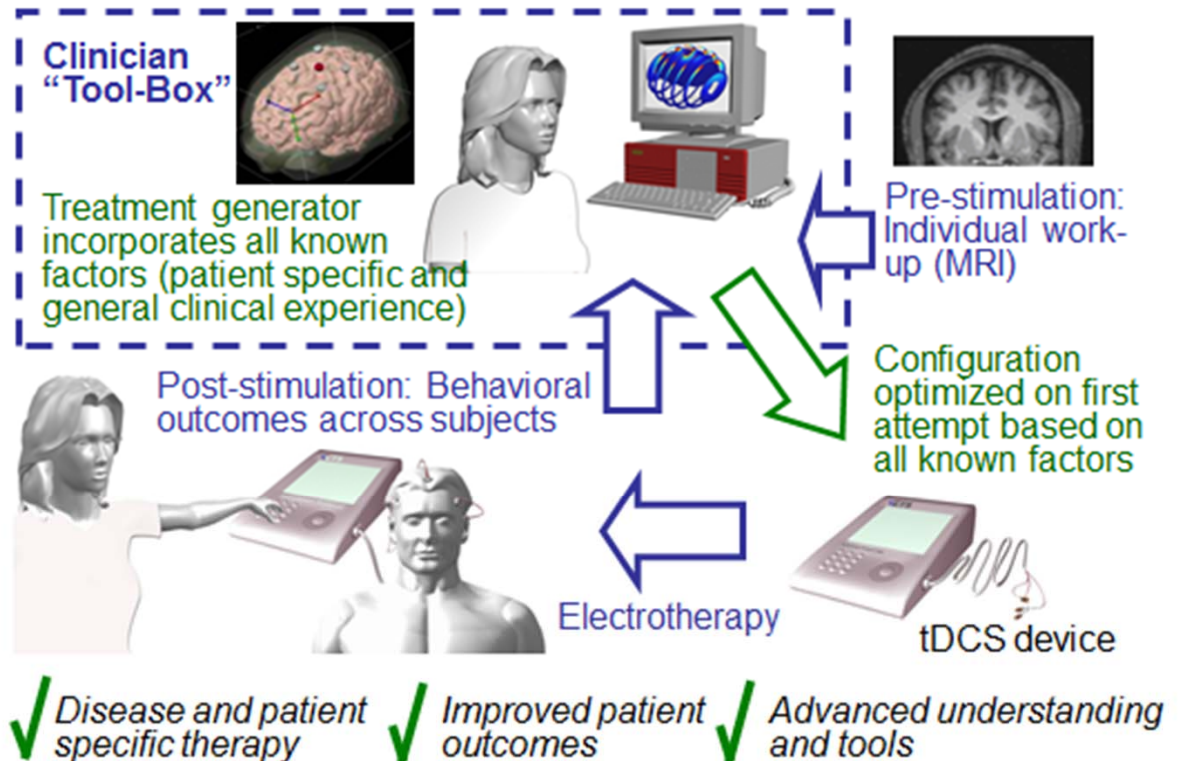
Best “guess” at stimulation configuration (from limited existing set)



Post-stimulation:
Behavioral outcomes

- X** Limited set of tDCS protocols used for highly disparate indications.
- X** No rational basis for patient specific considerations.
- X** Existing computational approaches not accessible (too time and computer resource intensive)

“Rational” electrotherapy design Patient and disease customized electrical therapy.



**If computational models can help
why are they not “popular”?**

**Limited access to simple and
cheap modeling**



Web-interface sufficient simple to use so that first-time users will not require instructions

Choose your setup from the following categories

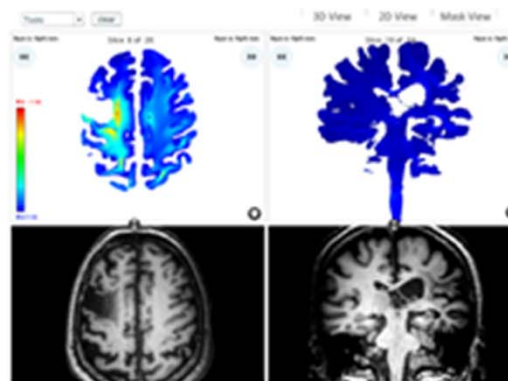
Basic Heads

These are normalized head examples. Start by choosing one of the following model types.



1

Simple flow-chart allows selection of "standard" heads or user-uploaded case studies

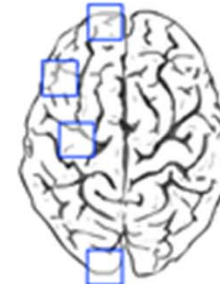


Simple navigation of resulting brain modulation in 2-D or 3-D space

Choose your setup from the following categories

Basic Heads

Now choose the **active** electrode (5cm by 5cm) location.



3

Electrode placement also entirely graphics driven

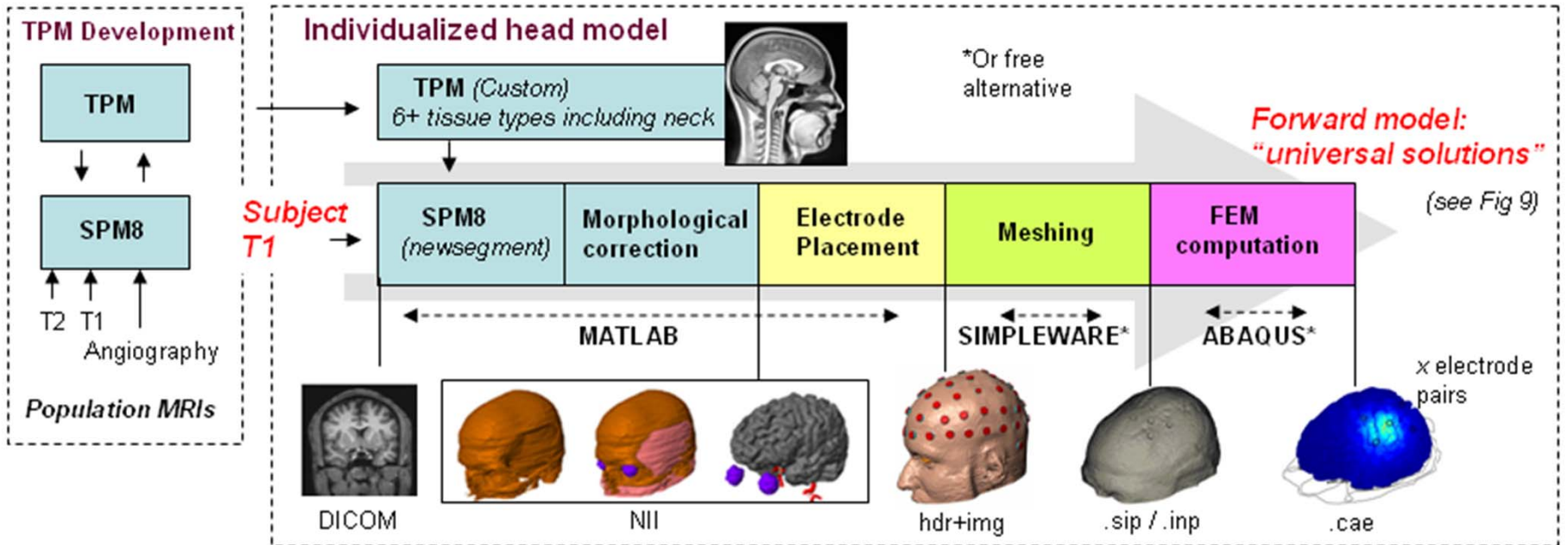
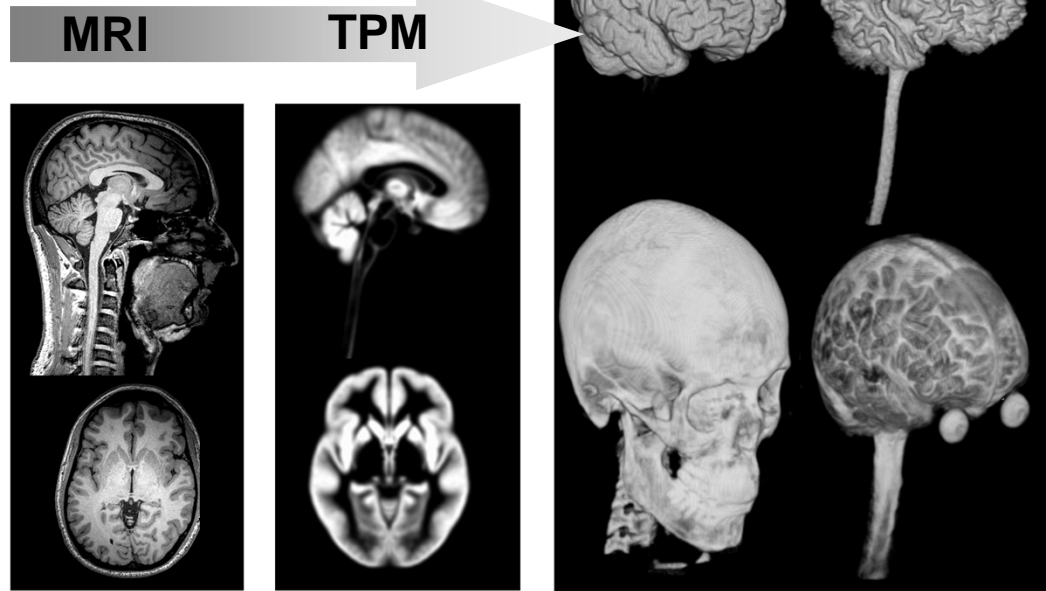
Now choose the **passive** electrode (5cm by 5cm) location.



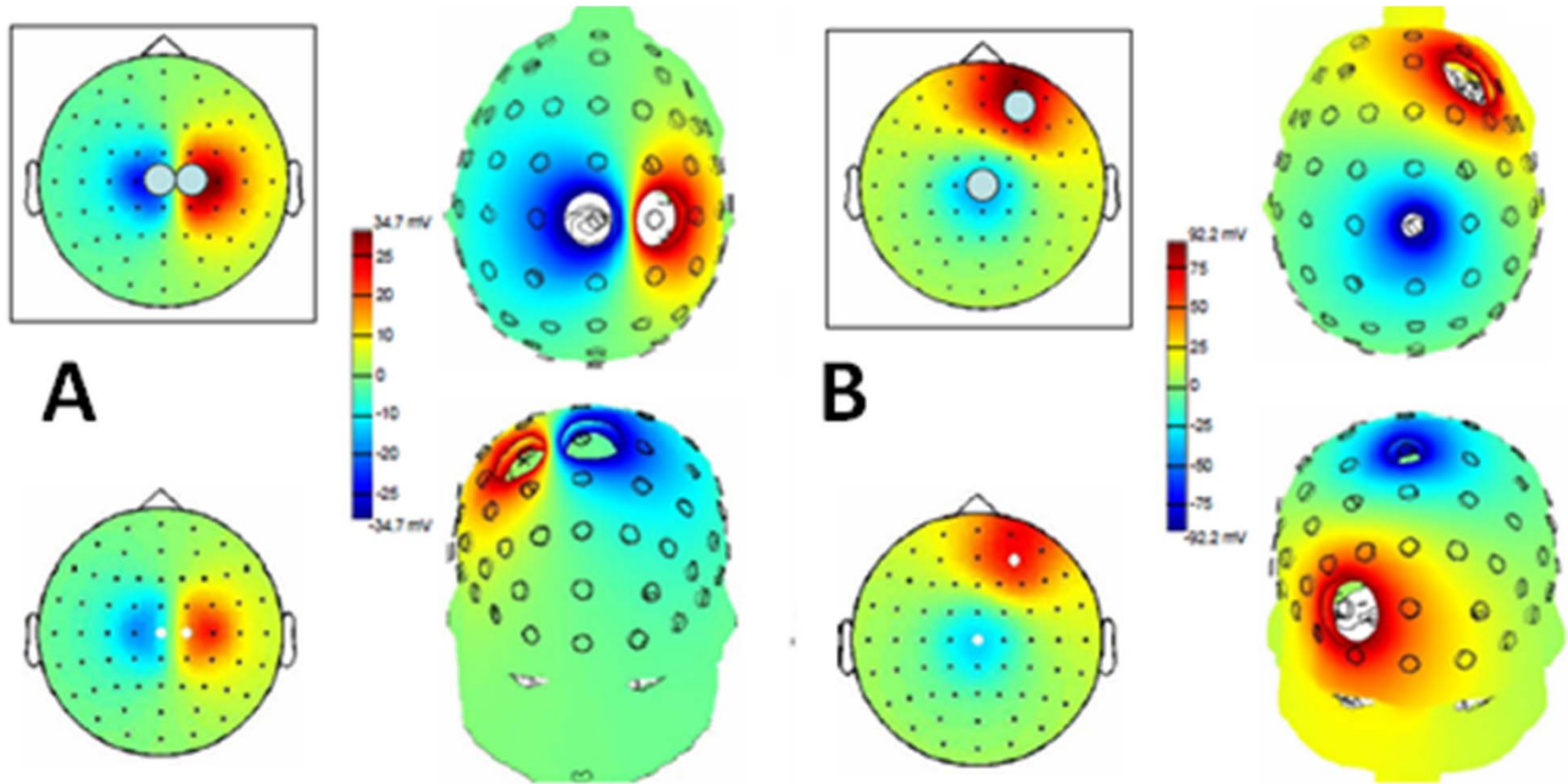
Neuralengr.com/Bonsai

Automated Work-Flow for Clinician Tool-Box

Automated high-accuracy head model for tDCS



Model Validation



Neuromodulation

- Application specific (neuropsychiatric, rehabilitation, cognitive performance...)
- Individualized therapy (customize, tune-able)
- Targeted brain modulation (space + time)
- Safe (reversible, minimal complications + counter-indications)
- Cost / Access (multi-use, production, treatment-infrastructure)

